



PAPER

Heart rate variability categories of fluctuation amplitude and complexity: diagnostic markers of fetal development and its disturbances

OPEN ACCESS

RECEIVED

22 January 2019

REVISED

29 April 2019

ACCEPTED FOR PUBLICATION

9 May 2019

PUBLISHED

28 June 2019

Original content from this work may be used under the terms of the [Creative Commons Attribution 4.0 licence](#).

Any further distribution of this work must maintain attribution to the author(s) and the title of the work, journal citation and DOI.



Dirk Hoyer¹, Alexander Schmidt¹, Kathleen M Gustafson², Silvia M Lobmaier³, Igor Lakhno⁴, Peter van Leeuwen⁵, Dirk Cysarz⁶, Hubert Preisl⁷ and Uwe Schneider⁸

¹ Hans Berger Department of Neurology, Biomagnetic Center, Jena University Hospital, Jena 07747, Germany

² Department of Neurology, Hoglund Brain Imaging Center, University of Kansas Medical Center, Kansas City KS66160, United States of America

³ Frauenklinik und Poliklinik, Klinikum rechts der Isar, Technische Universität München, München 81675, Germany

⁴ Kharkiv Medical Academy of Postgraduate Education, Kharkiv, Ukraine

⁵ Faculty of Health, University of Witten/Herdecke, Witten 58448, Germany

⁶ Integrated Curriculum for Anthroposophic Medicine and Institute of Integrative Medicine, University of Witten/Herdecke, Herdecke 58313, Germany

⁷ fMEG Center/Institute for Diabetes Research and Metabolic Diseases of the Helmholtz Center Munich at the University of Tübingen/ Germany, Center for Diabetes Research (DZD), Tübingen 72076, Germany

⁸ Department of Obstetrics, Division of Prenatal Diagnostics and Fetal Physiology, Jena University Hospital, Jena 07747, Germany

E-mail: Dirk.Hoyer@med.uni-jena.de

Keywords: heart rate variability, fetal development, developmental disturbance, prenatal diagnosis, diagnostic standard, clinical study

Abstract

Objective: In fetal diagnosis the myriad and diversity of heart rate variability (HRV) indices prevents a comparable routine evaluation of disturbances in fetal development and well-being. The work aims at the extraction of a small set of HRV key indices that could help to establish a universal, overarching tool to screen for any disturbance. **Approach:** HRV indices were organized in categories of short-term (prefix s) and long-term (prefix l) amplitude fluctuations (AMP), complexity (COMP), and patterns (PATTERN) and common representatives for each category were extracted. This procedure was done with respect to the diagnostic value in the evaluation of the maturation age throughout the second and complete third trimester of pregnancy as well as to potential differences associated with maternal life-style factors (physical exercise, smoking), nutrient intervention (docosahexaenoic acid (DHA) supplementation), and complications of pregnancy (gestational diabetes mellitus (GDM), intra-uterine growth restriction (IUGR)). **Main results:** We found a comprehensive minimal set that includes [lAMP: short term variation (STV), initially introduced in cardiotocography, sAMP: heart rate increase across one interbeat interval of phase rectified averaged signal - acceleration capacity (ACst1), lCOMP: scale 4 multi-scale entropy (MSE4), PATTERN: skewness] for the maturation age prediction, and partly overlapping [lAMP: STV, sAMP: ACst1, sCOMP: Lempel Ziv complexity (LZC)] for the discrimination of the deviations. **Significance:** The minimal set of category-based HRV representatives allows for a screening of fetal development and well-being. These results are an important step towards a universal and comparable diagnostic tool for the early identification of developmental disturbances.

Novelty & Significance

Fetal development and its disturbances have been reported to be associated with a multiplicity of HRV indices. Furthermore, these HRV indices change with maturation. We propose the abstraction of HRV categories defined by short- and long-term fluctuation amplitude, complexity, and pattern indices that cover all relevant aspects of maturational age, behavioral influences and a series of pathological disturbances. The study data are provided by multiple centers. Our approach is an important step towards the goal of a standardized diagnostic tool for early identification of fetal developmental disturbances with respect to the reduction of serious complications in the later life.

List of abbreviations and HRV parameters

For details and references of HRV indices see table 2.

2F	Fetal active sleep state
ANS	Autonomic nervous system
AUC	Area under curve
CI	Confidence interval
CTG	Cardiotocography
DHA	Docosahexaenoic acid
ECG	Electrocardiogram
fABAS	Fetal autonomic brain age score
FIGO	Fédération Internationale de Gynécologie et d'Obstétrique
GDM	Gestational diabetes melitus
HR	Heart rate
HRV	Heart rate variability
IUGR	Intrauterine growth restriction
MCG	Magnetocardiography
OGTT	Oral glucose tolerance test
r	Correlation coefficient
R ²	Coefficient of determination
ROC	Receiver operating characteristic
SD	Standard deviation
SE	Standard error
(W)GA	(Weeks) gestational age

HRV Parameters

Amp	Amplitude range: 20–95 inter quantile distance of detrended NN interval series
DCslx, DCstx, ACslx, ACstx	Deceleration capacity and acceleration capacity, slope and step value at coarse graining level x
DFA	Detrended fluctuation analysis: scaling indices α_1, α_2 EI _x —Ehler's index of temporal asymmetry at coarse graining level x
fABAS	Fetal autonomic brain age score
GI _x	Guzik's index of temporal asymmetry at coarse graining level x
HF	Fetal high-frequency band (0.4–1.7 Hz)
LF	Fetal low-frequency band (0.08–0.2 Hz)
LTV	Long-term variability
LZC	Lempel Ziv complexity of binary transformed NN intervals
mHR	Mean fetal heart rate
MSE _x	Generalized multiscale entropy at coarse graining level x
PI _x	Porta's index of temporal asymmetry at coarse graining level x
pNN5	Percentage of differences between adjacent NN intervals exceeding 5 ms
PRSA	Phase rectified signal averaging
PxV	Patterns with x variation of binary transformed NN intervals
RM	RMSSD—root mean square of successive NN interval differences
SD	SDNN—standard deviation of NN intervals
SE	Standard error
skew	Skewness
STV	Short-term variability
TP	Fetal total frequency power
VLF	Fetal very-low-frequency band (0.02–0.08 Hz)

Introduction

The focus *biological oscillations and health* addresses the essential role of fluctuations in the complex dynamic behavior of an organism. The formation of these fluctuations is an essential part of the phylogenetic evolution process and remains inherent in the ontogenetic maturation process (Haeckel 1866, Hoyer *et al* 2013b). Fetal developmental problems have irreversible implications for all of later life (Barker 1998, Van den Bergh *et al* 2017), but their early identification remains inadequate. In that context, characteristics of fetal heart rate patterns provide a unique diagnostic window during the

Table 1. Study centers and data.

Signal	Center location	Group	Number of available records	Number of analysed records 2F	Recording duration	WGA
MKG	Jena	Normal	567	484	30 min	18–40
		IUGR	48	34	30 min	26–38
	Bochum	Normal	305	296	5 min	15–42
		IUGR	78	49	5 min	19–40
	Tübingen	Normal	108	89	15 min	28–36
		GDM	39	31	15 min	28–36
	Kansas	Normal	19	12	18 min	36
		Exercise	21	15	18 min	36
	Kansas	Normal	68	60	2 × 18 min	24/32/36
		DHA	66	63	2 × 18 min	24/32/36
	Kansas	Pre-smoking	24	20	18 min	24/28/30/32/34/36/38
Post-smoking		24	17	18 min	24/28/30/32/34/36/38	
ECG	Kharkiv	Normal	74	45	10–30 min	20–36
		IUGR	13	5	10–30 min	20–36

second and third trimester of pregnancy (Nijhuis *et al* 1982, Pillai and James 1990, FIGO 2011). Various studies have addressed heart rate variability (HRV) indices of normal physiological fetal maturation as well as developmental disturbances, e.g. Van Leeuwen *et al* (1999), David *et al* (2007), Ferrario *et al* (2009) and Amorim-Costa *et al* (2017a, 2017b). Their results are generally consistent, but the dispersion of the results is high and the HRV indices used are diverse. This is partly caused by the variety of HRV indices available and simplified models with respect to the two (or more) influencing factors such as gestational age (GA) and physiological alterations. The sympathetic and parasympathetic branches of the autonomic nervous system (ANS) develop and mature at different rates. Consequently, developmental progression of fetal cardiac autonomic control can be measured by different HRV indices that reflect critical periods of ANS development across gestation (Schneider *et al* 2018). These developmental changes cannot be reflected by linear models which assume a constant development across the total second and third trimester. Furthermore, the diversity of HRV indices suggests high accuracy, but it rather leads to statistically over-fitted models and physiological over-interpretations. Based on the redundancy of the multiplicity of HRV indices, identifying a few relevant key parameters would help to propose a feasible, universally manageable and standardized diagnostic tool for early identification of fetal developmental disturbances with a view to the reduction of serious complications in later life.

The myriad different HRV indices applied in individual studies hinders easy and reliable comparisons of methods and results. Some of the indices are redundant, and others discriminative only with respect to particular influences or disturbances (TaskForce 1992, Stein 2005, Maestri *et al* 2007, Schmidt *et al* 2018b). Within categories of HRV amplitude, complexity, and heart rate patterns, respectively, we expect certain redundancies between the category members. It is our intention to introduce and evaluate a concept that significantly reduces the number of HRV indices without losing the option of integrating novel indices while remaining appropriate for the identification of additional, not yet considered alterations of autonomic control.

The aim of the present work is to identify key HRV categories that reflect physiological development of the fetal ANS with respect to important maturational periods during the second and third trimester. The diagnostic value of these categories is explored using several examples of maternal and fetal factors that have previously been shown to influence fetal HRV. Representatives of these key HRV categories are proposed as universal, overarching candidates for fetal screening and could be an important step towards a standardized diagnostic tool.

Methods

Subjects and recordings

From the recordings provided by the following centers, only sections of active sleep (2F) lasting at least 7 min, generally 10 min, were analysed; for an overview see table 1. Only the 5 min data sets from Bochum were analysed regardless of state, as they were too short for state selection.

Normal group

MCG recordings lasting 30 min from the Jena study data base (Biomagnetic Center/Department of Neurology, Department of Obstetrics/Division of Prenatal Diagnostics and Fetal Physiology, Jena University Hospital). For methodological details, see e.g. Hoyer *et al* (2013b).

Normal reference group

MCG recordings lasting 5 min from the Bochum study data base (Grönemeyer Institute for Microtherapy, University Witten/Herdecke, Bochum). For methodological details see Hoyer *et al* (2015).

Effect of maternal exercise

Healthy women with low-risk, singleton pregnancies gave informed consent and were enrolled in a study designed to determine the effect of maternal physical activity on fetal cardiac autonomic control. Women were categorized into exercise or control groups based on self-report to a standardized questionnaire. MCG recordings lasting 18 min were recorded at 24, 32 and 36 WGA (Hoglund Brain Imaging Center, Department of Neurology, University of Kansas Medical Center, Kansas City, Kansas, USA). Twenty-one women were assigned to the exercise group and 19 women to the control group. Differences in fetal HRV were found only at 36 WGA, therefore this analysis is limited to fetal data recorded at that time point. For details of the parent study, see May *et al* (2010). Data used in this report were obtained from available public data (Van Leeuwen *et al* 2014a).

Effect of maternal smoking

Healthy pregnant women ($n = 24$) with low-risk, singleton pregnancies who reported smoking during pregnancy gave informed consent and enrolled in a study designed to measure the effect of maternal smoking on fetal HRV. Women abstained from smoking overnight. MCGs of 18 min duration were recorded prior to and immediately after smoking their first cigarette of the day (pre- versus post-smoking) at 24, 28, 32, 34, 36 and 38 WGA. (Hoglund Brain Imaging Center, Department of Neurology, University of Kansas Medical Center, Kansas City, Kansas, USA)

Influence of maternal docosahexaenoic acid (DHA) supplementation

Following informed consent, healthy pregnant women ($n = 67$) with low-risk, singleton pregnancies enrolled in a randomized clinical trial (NCT01007110) designed to test the effect of DHA supplementation on fetal cardiac autonomic control. Women consumed daily capsules containing a mixture of corn/soy oil (placebo) or 600 mg of DHA during the last two trimesters of pregnancy. MCGs of 18 min duration were recorded at 24, 32 and 36 weeks WGA at the Hoglund Brain Imaging Center, Department of Neurology, University of Kansas Medical Center, Kansas City, Kansas, USA. For methodological details of the parent trial see Gustafson *et al* (2013). Significant differences in fetal HRV were reported at 32 and 36 WGA. For this report, we used data from 32 WGA (24 placebo; 23 DHA) and 36 WGA (19 placebo; 21 DHA).

Influence of IUGR: MCG recordings from IUGR fetuses (estimated weight < 10th percentile with respect to GA, pathological uteroplacental perfusion > 24 WGA) versus normal group from the Jena study data base.

Influence of IUGR reference group 1

MCG recordings from the Bochum data base and respective normal controls. For details see Hoyer *et al* (2015).

Influence of IUGR reference group 2

Fetal non-invasive ECG recordings obtained from maternal abdominal surface were performed in the Kharkiv perinatal center. The methodology has been previously described (Hoyer *et al* 2017). Since the extraction of high-quality beat-to-beat variability using fetal ECG is still a challenge (see e.g. van Leeuwen *et al* (2014b)), a total quantity of performed records were twice higher. Tracings with sufficient quality were found predominately in the periods from 20 to 28 weeks and from 34 to 36 weeks of gestation. Therefore, this peculiarity could have an influence on the fetal gestational age distribution in fetal ECG cohort.

Influence of gestational diabetes mellitus (GDM)

GDM is defined by increased glucose levels during an oral glucose tolerance test OGTT, (500 ml drink containing 75 gr sugar). We recorded data in 13 pregnant women with GDM and 36 pregnant women with normal glucose tolerance. The participants were recorded three times, directly before intake of the solution and 60 and 120 min after ingestion of the glucose (for methodological details see Fehlert *et al* (2017) and Cysarz *et al* (2013)).

Inclusion criteria

Fetal heart rate recording in sinus rhythm of singletons during the second and third trimester, maternal age > 18 year, approval from the associated local Ethics Committees and written consent of the participants.

Gestational ages were calculated from the date of the last menstrual period and confirmed by first trimester crown-rump-length measurement.

Exclusion criteria (normal groups and controls in clinical cohorts)

Maternal: known heart disease, medication affecting cardiac function, smoking, abuse of alcohol or illicit drugs, diabetes mellitus (both pre-pregnancy Type I/II and gestational diabetes).

Fetal: known chromosomal abnormalities, sonographically identified malformations, uterine contractions during recording, cardiac arrhythmias, IUGR (normal groups), previous exposure to synthetic steroids for premature induction of lung maturation.

Fetal behavioral states

The fetal behavioral state is a fundamental factor of autonomic activity and HRV. In order to keep the present work clear, we report only results during active fetal sleep (2F) according to CTG standards that propose to use an active state in order to exclude adverse behavior or developmental disturbances (FIGO 2011). The states of all data sets were classified from visual inspection of the heart rate pattern printout after a consensus decision by three independent obstetricians of the Jena study center.

HRV indices and categories

The HRV indices used include the most common ones and were organized according to their signal processing origin into categories of amplitude, complexity and patterns (table 2). All HRV indices were calculated from preprocessed NN interval series after removal of artifacts and decelerations according to previous analyses (Hoyer *et al* 2014, Schmidt *et al* 2018a). Recordings were considered only if less than 5% of their time length had been corrupted by artifacts. The distributions of the HRV indices were tested for normality via the Shapiro–Wilk test and the visual inspection of the QQ-plot. In order to ensure a normal distribution of the HRV indices, different transformations functions (sqrt/log) were used. The signal analysis was done using MatLab2014a.

Categories of HRV indices were established with respect to their physiologic and system-theoretic origin and their correlations in the normal group. According to the linear nature of the amplitude indices we proposed a short-term category which is predominantly related to vagal activity and a long-term category that reflects both, vagal, sympathetic and humoral modulations. Complexity is a nonlinear property across less clearly separable time scales. We included all complexity indices in one category, however provided a short-term and a long-term index where appropriate. The category of patterns contains different approaches like skewness and power-ratios. Furthermore, for each multi-scale temporal asymmetry index a short-term and a long-term proxy were considered (overview see table 2).

Statistical analysis

The gestational age range was divided into overlapping age windows, namely: range 23 (20–26), range 26 (23–29), range 29 (26–32), range 32 (29–35), and range 35 (32–38) WGA. The dependency between each of the HRV category representatives and the chronological fetal age in each window was estimated by linear regression models (standardized beta coefficient β , 95% CI). The partial Spearman's rank correlation coefficients between the HRV indices of the Jena normal group (2F) were calculated partialized to GA in order to remove the confounding effect of GA.

The GA dependencies/prediction were compared by linear regression models, quantified by the mean standard error (SE) and coefficient of determination R^2 in a 3-fold cross-validation-scheme with 10 repeats. The SE's from the single folds are tested via Wilcoxon signed rank sum test for significant differences. The groups were compared by logistic regression models, quantified by the mean area under the curves (AUC) value of the receiver operating characteristic (ROC) in a three fold cross-validation-scheme with 10 repeats. The AUC's from the single folds are tested via Wilcoxon signed rank sum test for significant differences. The further group comparisons were done using Wilcoxon–Mann–Whitney U Test and the paired groups by Wilcoxon signed rank test (*R* version 3.3.2). OGTT was analyzed by two-factorial variance analysis of repeated measures (IBM SPSS statistics 25). The significance level α was set to 0.05

Investigation flow

1. Representatives of categories with respect to normal fetal aging
 - a. Validation of categories by correlation matrix of the Jena normal group.
 - b. Select a representative (best age predictor) HRV index for each category.
 - c. Check for synergism by investigation the best couple of HRV indices (age prediction).
2. Representatives of categories with respect to identification of different deviations (see 4.b)
 - a. Evaluation of the discriminatory value of the representatives.
(comparison of age representatives from 1b with best discriminators and the best discriminating couple of HRV indices separately for the particular deviations).
 - b. Select a set of representatives with discriminatory value across all kind of deviations in comparison with the best ones of each particular deviation.

Table 2. HRV categories of short and long term amplitude/magnitude ‘AMP’, complexity ‘COMP’, and different patterns ‘PATTERN’. ‘l’ and ‘s’ are indicators for long term and short term versions (as used here for AMP, but also for other categories below).

AMP: magnitude (amplitude): indices of the range of fluctuations dependent on different time resolutions or frequency bands		
Short	RM: RMSSD-root mean square of successive beat differences	TaskForce (1996)
(sAMP)	pNN5: percentage of successive NN intervals greater than 5 ms	TaskForce (1996)
	HF (high frequency band power)	David et al (2007)
	P0V, P1V, P2V: percentage of no, one, or two respective changes in a binary series of successive NN intervals	Cysarz et al (2015) and Cysarz et al (2013)
	DCsl1, DCst1, ACsl1, ACst1: slope and step values of heart rate deceleration and acceleration capacity across 1 NN interval change (short) after PRSA (phase rectified signal averaging)	Bauer et al (2006) and Lobmaier et al (2012)
Long	SD: SDNN -standard deviation of NN intervals	TaskForce (1996)
(lAMP)	TP: total power, VLF: very low frequency p , LF: low frequency p	David et al (2007)
	Amp: 20-95 inter-quantile range of NN intervals	
	STV: mean difference between consecutive NN interval epochs of 3.75 s, w/o DC, artifacts <50%, the parameter is referred to as STV—‘short term variation’ in the literature owing to the temporal resolution constrains of cardiocography	Pardey et al (2002)
	LTV: ‘long-term variation’, mean fluctuation range of NN epochs in 1 min sections w/o DC, artifacts < 50%, part of the dataset referred to as the Dawes-Redman-criteria	Pardey et al (2002)
	DCsl4, DCst4, ACsl4, ACst4, slope and step values across the change at a coarse graining level of 4 NN intervals (long)	See above
COMP: complexity: indices of irregularity, invers to predictability. Complexity is a characteristic that is per definition independent of the amplitude of a signal		
LZC: Lempel Ziv complexity (short)		Lempel and Ziv (1976)
MSE: multi-scale entropy, calculated from generalized mutual information from original NN series, scale 1 (short), scale 4 (long), equivalent to approximate entropy and sample entropy		Richman and Moorman (2000) and Hoyer et al (2013a)
$\alpha 1$: fractal scaling index: across 4–11 NN (short), $\alpha 2$:—across > 11 NN intervals (long) from DFA (Detrended Fluctuation Analysis)		Peng et al (1995)
PATTERN: indices derived from nonlinear distributions or ratios. They are in the most cases per definition independent of the amplitude or complexity of the original signal		
skew: skewness (third statistical moment, asymmetry of the probability distribution of a random variable such as NN interval series)		
VLF/LF, VLF/HF, LF/HF (ratios of frequency band power)/SD/RM: SDNN/RMSSD (corresponding ratio of time domain indices)		David et al (2007) and Schneider et al (2008)
Multiscale temporal asymmetry (short scale 1, long scale 4)		Porta et al (2008)
PI1, PI4 (Porta’s index, percentage of negative values in the [NN(i), NN(i + 1)] map normalized to the total number of values)		
GI1, GI4 (Guzik’s index, cumulative distance of [NN(i), NN(i + 1)] values above the main diagonal normalized to the overall cumulative distance)		
EI1, EI4 (Ehler’s index, skewness of [NN(i), NN(i + 1)] distribution)		

3. Propose a minimal set of HRV key indices for screening of autonomic maturation age and all kinds of deviations.
4. Application of minimal set
 - a. Assessment of maturation age across 2nd and 3rd trimester.
 - b. Identification of deviations due to maternal life-style factors (physical exercise, smoking), nutrient intervention (docosahexaenoic acid (DHA) supplementation), and complications of pregnancy (gestational diabetes mellitus (GDM), intra-uterine growth restriction (IUGR)).

Results

Representatives of categories with respect to normal fetal aging

The correlation matrix (figure 1) mainly confirms the proposed category members. mHR shows weak correlations with parameters of lAMP and sAMP. In lAMP (AMP, SD, STV, LTV, TP, VLF, LF, ACsl4, ACst4, DCsl4, DCst4) and sAMP (pNN5, RM, P0V, P1V, P2V, HF, ACsl1, ACst1, DCsl1, DCst1), respectively, all members were clearly correlated with correlation coefficients r of about 0.7 to 1.0. In the lAmp category, the lowest correlation

coefficient $r = 0.55$ was observed between Amp and Dcsl4 and in the sAmp category, the lowest correlation was found between P1V and ACst1 ($r = 0.46$). Herein, all PRSA related indices were mutually correlated as well as with sAMP and lAMP members ($r = 0.6-0.9$). Weaker correlations ($r \approx 0.5$) could be observed between sAMP and lAMP members.

Concerning short scale members of the COMP category LZC and MSE1 were not correlated. Overall, LZC shows negligible correlations with all other parameters. However, MSE1 and $\alpha 1$ were correlated ($r = 0.76$) as short scale members as well as MSE4 and $\alpha 2$ ($r = 0.79$) as long scale members. Furthermore, MSE1 and $\alpha 1$, respectively, show correlations ($r \approx 0.8$) with the themselves strongly correlated pattern related indices VLF/HF, LF/HF and SD/RM.

In the PATTERN category, the different aspects like skewness, sympatho-vagal balance (VLF/LF, LF/HF, SD/RM, LF/HF), and time irreversibility (P^* , G^* , E^*) were not correlated. However, the three Asym indices were mutually correlated at similar time scales (P1-G1; $r = 0.68$, E1-G1: $r = 0.88$, P4-G4: $r = 0.50$, E4-G4: $r = 0.82$). Inside the sympatho-vagal balance parameters VLF/LF seems to stand alone in comparison the other three.

In order to check for the exclusivity of the selected representatives of categories we compared the standard errors of the best age-predicting representatives with the best predicting couple. The improvements of SE were less than 0.1 WGA and, hence, irrelevant compared to the clinical precision of the age determination with a confidence interval of ± 1 WGA ((Geirsson 1991), table 3). SE of COMP was decreased by 0.5 towards 3.7 in the combination of MSE4 and $\alpha 2$. Therefore, we used only MSE4 for that category as candidates for the minimal set.

Representatives of categories with respect to identification of different deviations

It was our intention to find an appropriate minimal set of category representatives that allows the identification of all investigated deviations. Table 4 shows, that the best deviation class discriminating indices were significantly different compared to the age prediction representatives. However, the improvements by using couples of indices were mainly below an AUC difference of 0.05 and could primarily be reached in investigations at younger ages, like in DHA (24 WGA) and IUGR (both in Jena and Bochum before 32). In studies after or around 32 WGA, nearly no significant improvements could be reached. Accepting this minor loss of precision at the younger ages, a minimal screening set could be established by just one representative per category. For this objective, the same representatives across all kinds of deviations are required. The AUC values of the respective set [ACst1, STV, LZC] we reduced by a maximum of 0.06 in comparison to the best results. Therefore, we did not include any of them in the minimal set.

Minimal set for overarching screening of maturation age and deviations

While maturation age was related to both [Amp, pNN5, MSE4, skew], all investigated deviations could be screened for by at least one of [ACst1, STV, LZC].

Since ACstep1 and pNN5 predict maturation age almost similarly (table 3), but ACstep1 better discriminated most of the deviation aspects (table 4), we propose ACstep1 as overarching representative of sAMP.

STV and Amp predict maturation age almost similarly (table 3), but STV better discriminated most of the deviation aspects (table 4). Furthermore, STV is common in established CTG analysis and allows the transfer of results obtained by MCG to the established CTG recordings and standards. Therefore, we propose STV as overarching representative of lAMP.

Because LZC did not significantly predict age we propose to keep MSE4 as (lCOMP) age predicting feature while LZC as (sCOMP) classification feature representative.

The resulting overarching minimal set includes [STV, ACst1, MSE4, skew] for the maturation age prediction and [STV, ACst1, LZC] for the discrimination of other deviations.

Assessment of maturation age across 2d and 3d trimester by minimal set [STV, ACst1, MSE4, skew]

The results shown in figure 2 indicate that the most profound maturation related changes appeared up to the investigation range of (26–32) WGA, namely increasing values (positive regression coefficients) of lAMP, sAMP, lCOMP indices and the pattern index skewness. In contrast, after a transition period at the range of (29–35) WGA, the indices of both AMP categories become again strong predictors, but the COMP and pattern index lose their relevance.

The Bochum data qualitatively confirm these results. Lower significances can be explained by the higher variability of the state-independent and shorter (5 min) recordings.

Assessment of deviations by influencing factors by minimal set [STV, ACst1, LZC]

In table 5, significant changes due to influencing factors are shown. The corresponding statistical metrics are given in table 4. Please note that the data sets were obtained by availability. Consequently, we were not able to investigate the different influencing factors for all developmental periods. Nevertheless, we found systematic examples of significant discriminatory power for each HRV category.

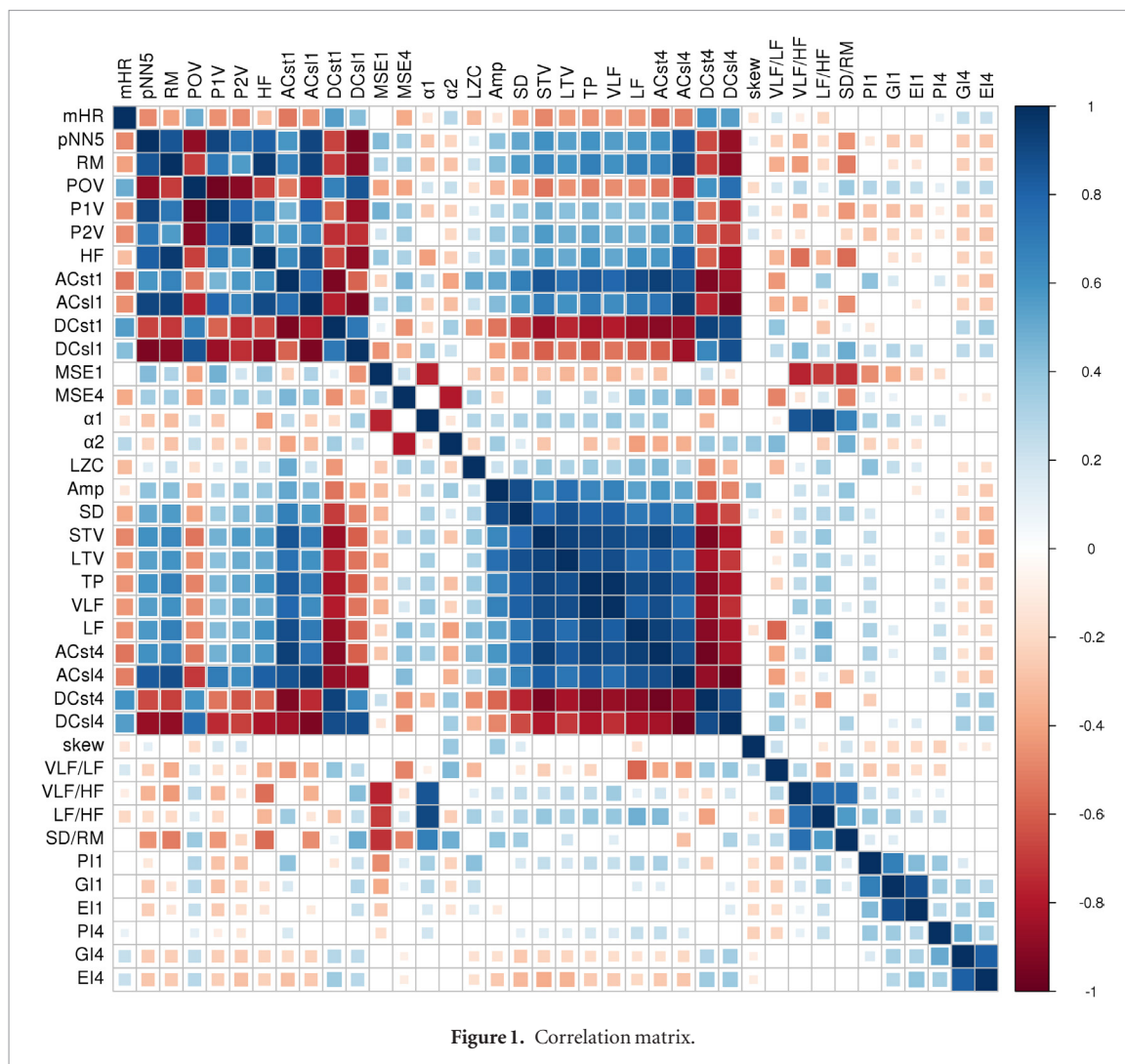


Figure 1. Correlation matrix.

Table 3. Standard errors SE(standard deviation SD of SE)/coefficient of determination R^2 in WGA of minimal set members of classifiers extracted below, best single and best couple of age predicting indices.

Category	Classification feature representative SE(SD)/ R^2	Best age predicting feature SE(SD)/ R^2	Best age predicting couple SE(SD)/ R^2
Jena (18–40 WGA)			
sAMP	3.89(0.13)/0.26 (ACst1)	3.67(0.15)/0.35 (pNN5) ^a	3.57(0.16)/0.38 (pNN5 + RM) ^b
IAMP	3.83(0.14)/0.29 (STV)	3.55(0.14)/0.39 (Amp) ^a	3.46(0.16)/0.42 (AMP + DCs14) ^v
COMP	4.49(0.11)/0.02 (LZC)	4.21(0.15)/0.13 (MSE4) ^a	3.70(0.18)/0.34 (MSE4 + α_2) ^b
Patterns		3.82(0.15)/0.29 (skew)	3.77(0.16)/0.31 (skew + VLF/HF) ^b
Bochum (15–42 WGA)			
sAMP	5.38(0.28)/0.34 (ACst1)	4.98(0.33)/0.43 (POV) ^a	4.93(0.31)/0.44 (pNN5 + DCs11) ^b
IAMP	5.74(0.23)/0.24 (STV)	5.15(0.31)/0.39 (DCs14) ^a	5.10(0.26)/0.41 (STV + DCst4)
COMP	6.24(0.20)/0.11 (LZC)	5.78(0.31)/0.24 (MSE4) ^a	5.54(0.32)/0.30 (MSE4 + α_2) ^b
Patterns		5.74(0.28)/0.24 (skew)	5.33(0.29)/0.35 (skew + VLF/HF) ^b

^a Indicates significant difference between best single age predictor and classification representative.

^b Indicates significant difference between best single and couple age predictor.

Compared to the results in the above section on age dependency, we did not find a general change from predominantly discriminating HRV complexity and amplitude before 32 WGA to a solely predominantly discriminating HRV amplitude after 32 WGA. However, it is important to note that there seems to be a dominance of amplitude changes due to maternal life-style factors (physical exercise, smoking) in contrast to both amplitude and complexity changes in connection with fetal growth (IUGR) and nutrient supplementation (DHA).

Table 4. Classification results: area under curve (AUC) and 95% confidence interval (CI) per category: age prediction representative versus best classifiers versus best predicting couple, minimal set of overarching classifiers.

Category	Age predicting feature representative	Classification feature representative	Best classification feature	Best classification couple
Physical exercise (36 WGA)				
sAMP	.70(.65–.75)(pNN5)	.75(.70–.80)(ACst1)	.75(.70–.80)(ACst1) ^a	.70(.66–.75)(HF + ACst1) ^b
IAMP	.78(.74–.83)(Amp)	.77(.73–.81)(STV)	.83(.83–.87)(VLF)	.85(.81–.89)(VLF + DCst4)
COMP	.35(.31–.38)(MSE4)	.68(.62–.75)(LZC)	.71(.66–.75)(MSE1) ^a	.66(.61–.71)(MSE4 + α 1)
PATTERN	.33(.27–.39)(skew)		.62(.55–.70)(PI4) ^a	.70(.65–.75)(GI4 + EI4) ^b
DHA supplement (24 WGA)				
sAMP	.38(.33–.42)(pNN5)	.45(.40–.50)(ACst1)	.45(.40–.50)(ACst1) ^a	.57(.52–.63)(pnn5 + P0V) ^b
IAMP	.39(.35–.43)(Amp)	.41(.38–.45)(STV)	.52(.47–.57)(LF) ^a	.59(.53–.65)(STV + LF) ^b
COMP	.56(.49–.63)(MSE4)	.37(.34–.41)(LZC)	.56(.49–.63)(MSE4)	.60(.55–.65)(MSE4 + α 2)
PATTERN	.59(.53–.64)(skew)		.67(.64–.71)(EI4) ^a	.70(.66–.73)(EI1 + EI4)
DHA supplement (32 WGA)				
sAMP	.73(.69–.78)(pNN5)	.74(.69–.79)(ACst1)	.80(.76–.83)(P2V) ^a	.78(.74–.82)(RM + P2V)
IAMP	.55(.51–.60)(Amp)	.71(.67–.76)(STV)	.75(.71–.80)(DCsl4)*	.74(.70–.79)(DCst4 + DCsl4)
COMP	.67(.60–.73)(MSE4)	.77(.73–.82)(LZC)	.77(.73–.82)(LZC) ^a	.76(.76–.81)(LZC + α 1)
PATTERN	.46(.42–.51)(skew)		.57(.51–.63)(PI4) ^a	.60(.56–.64)(PI4 + EI4)
DHA supplement (36 WGA)				
sAMP	.68(.64–.73)(pNN5)	.71(.67–.76)(ACst1)	.74(.69–.78)(P2V) ^a	.74(.70–.78)(P1V + P0V)
IAMP	.76(.73–.80)(Amp)	.72(.67–.76)(STV)	.82(.79–.85)(SD) ^a	.80(.77–.84)(Amp + SD)
COMP	.43(.38–.48)(MSE4)	.69(.64–.73)(LZC)	.69(.64–.73)(LZC) ^a	.70(.66–.74)(MSE4 + LZC)
PATTERN	.44(.40–.48)(skew)		.60(.55–.65)(PI4) ^a	.62(.58–.67)(SD/RM + PI4)
IUGR (Jena, < 32 WGA)				
sAMP	.42(.38–.47)(pNN5)	.71(.67–.74)(ACst1)	.71(.67–.74)(ACst1) ^a	.78(.76–.80)(P2V + DCsl1) ^b
IAMP	.51(.45–.57)(Amp)	.72(.68–.76)(STV)	.73(.70–.77)(ACst4) ^a	.77(.72–.77)(DCst4 + DCsl4) ^b
COMP	.65(.61–.68)(MSE4)	.75(.72–.78)(LZC)	.75(.72–.78)(LZC) ^a	.75(.73–.79)(LZC + α 2)
PATTERN	.44(.41–.48)(skew)		.69(.66–.73)(LF/HF)*	.69(.58–.62)(VLF/HF + SD/RM)
IUGR (Jena, \geq 32 WGA)				
sAMP	.66(.62–.69)(pNN5)	.69(.67–.72)(ACst1)	.69(.67–.72)(ACst1)*	.70(.67–.72)(RM + HF)
IAMP	.67(.65–.70)(Amp)	.76(.73–.79)(STV)	.76(.73–.79)(STV) ^a	.76(.73–.78)(STV + TP)
COMP	.58(.53–.62)(MSE4)	.59(.54–.64)(LZC)	.59(.54–.64)(LZC)	.61(.57–.64)(MSE1 + MSE4)
PATTERN	.58(.54–.62)(skew)		.63(.60–.66)(PI1) ^a	.68(.65–.72)(PI1 + EI1) ^b
Bochum (Jena, < 32 WGA)				
sAMP	.51(.47–.56)(pNN5)	.60(.56–.64)(ACst1)	.60(.56–.64)(ACst1) ^a	.73(.71–.75)(P2V + ACsl1) ^b
IAMP	.54(.51–.58)(Amp)	.60(.56–.64)(STV)	.66(.63–.70)(VLF) ^a	.77(.74–.80)(Amp + TP) ^b
COMP	.53(.47–.59)(MSE4)	.47(.44–.50)(LZC)	.67(.62–.71)(α 2) ^a	.64(.60–.68)(MSE1 + α 2) ^b
PATTERN	.64(.61–.66)(skew)		.72(.69–.75)(EI1) ^a	.75(.72–.77)(SD/RM + EI1)
Bochum (Jena, \geq 32 WGA)				
sAMP	.64(.60–.67)(pNN5)	.63(.61–.66)(ACst1)	.67(.64–.71)(P1V) ^a	.65(.62–.69)(HF + ACsl1)
IAMP	.50(.46–.54)(Amp)	.55(.51–.58)(STV)	.64(.60–.67)(DCsl4) ^a	.67(.64–.69)(VLF + TP)
COMP	.59(.55–.62)(MSE4)	.49(.45–.52)(LZC)	.62(.59–.65)(MSE1)	.61(.57–.64)(α 1 + α 2)
PATTERN	.57(.54–.60)(skew)		.67(.65–.70)(VLF/HF) ^a	.68(.66–.71)(skew + VLF/HF)
Pre-post smoke				
sAMP	.26 (pNN5)	.16 (ACst1)	.08 (RM)	—
IAMP	.23 (Amp)	.05 (STV)	.05 (STV)	—
COMP	.67 (MSE4)	.48 (LZC)	.48 (LZC)	—
PATTERN	.21 (skew)		.21 (skew)	—
OGTT				
sAMP	.013/.407 (pNN5)	.010/.348 (ACst1)	.002/.193 (HF)	—
IAMP	n.s. (Amp)	.002/.123 (STV)	.060/.056 (LF)	—
COMP	.026/.238 (MSE4)	n.s. (LZC)	.001/.734 (MSE1)	—
PATTERN	n.s. (skew)		.016/.067 (MSE5)	—
			.001/.276 (VLF/HF)	—

^a Indicates significant difference between best single classification feature and the best age predicting feature.^b Indicates significant difference between best single and couple of classification feature. OGTT: significances of differences and interactions.

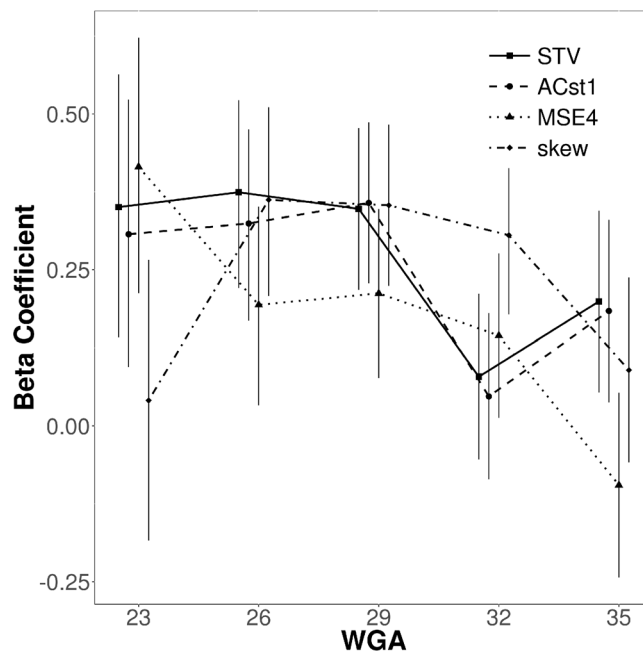


Figure 2. Normal group of Jena data base, linear regression models describing HRV categories by fetal WGA, standardized regression coefficient Beta, 95% CI of GA intervals: range 23 (20–26), range 26 (23–29), range 29 (26–32), range 32 (29–35), range 35 (32–38).

Discussion

The myriad and diverse published HRV indices prevent their standardized application in routine clinical evaluation of fetal maturation, its pathophysiological disturbances as well as of behavioral influences. The present work aimed at the extraction of a clear set of a few HRV representatives capable for an overarching monitoring/screening of as many of those aspects as possible. All familiar HRV indices were organized in categories according to physiological and signal-theoretical aspects and the members of each category were checked for redundancies and synergism with respect to physiological maturation age and deviations from the normal values.

Across all aspects of deviations we suggest overlapping sets of [IAMP(STV), sAMP(ACst1), lCOMP(MSE4), PATTERN(skewness)] for maturation age prediction and [IAMP(STV), sAMP(ACst1), sCOMP(LZC)] for the discrimination.

It is remarkable that only in a few cases multivariate intra-category models weakly improved the predictive value of particular deviations. This was mainly the case when considering fetuses below 32 WGA and could be an expression of more complex system behavior and development during this period. This could be of interest in subsequent diagnosis in more detail after identification of suspect cases using the overarching screening methodology presented here. However, with respect to the screening we could not find overarching multivariate intra-category models. The merging of categories was no option since they consider different aspects of physiological system behavior.

In the present work we found changing relevance of HRV indices with respect to the GA with a transition range around 32 WGA (29–35 WGA). In terms of nonlinear dynamics, this phenomenon can be interpreted as a typical phase transition period where the signal becomes less clearly assignable at the edge between the previous and the subsequent maturation period. Also, from a physiological point of view, the change from the predominant formation and growth of vagal and sympathetic complex structures before 32 WGA towards the increase of behavioral patterns of the mainly developed complex organism after 32 WGA indicates a phase transition. A corresponding transition range has been reported in the development of the HRV power spectra and complexity indices (Van Leeuwen *et al* 2003, Hoyer *et al* 2017). In a previous study using a former recruitment state of the Jena data base of 312 recordings from 60 women using multivariate linear mixed models over four maturation segments (<27, 27–31, 31 + 1–35, >35 + 1 WGA) we found qualitatively similar relationships of corresponding HRV indices (Schneider *et al* 2018). The previously described components of fABAS found by linear regression, namely Amp, pNN5, MSE3, skew (Hoyer *et al* 2013b) perfectly fit with the category representatives elaborated in this study: IAMP: Amp \approx STV, sAMP: pNN5 \approx ACst1, lCOMP: MSE4, PATTERN: skew. A similar analysis applied to the independent Bochum 5 min normal group recordings confirmed the main characteristics of the HRV categories.

The examples of deviations investigated are the result of our international search for appropriate data sets with heart rate patterns of MCG quality. The data sets were independent between the study centers but constitute only an incomplete survey.

Table 5. HRV categories representatives significantly associated with the influencing factors: ↑/↓ : significant increase/decrease compared to normal group due to corresponding factor, —: no association, empty fields: no data. The corresponding quantitative statistics in detail are given in the table 4.

HRV category versus influencing factor	20–32 WGA				Range 32 (29–35) WGA				32–38 WGA			
	HR	sAMP	IAMP	COMP	HR	sAMP	IAMP	COMP	HR	sAMP	IAMP	COMP
Physical exercise 36 WGA									—	↑	↑	—
DHA supplement. 32WGA 36WGA					—	↑	↑	↑	—	↑	↑	↑
IUGR, Jena	↑	↓	↓	↓	(↑) 0.07	↓	↓	↓	↑	↓	↓	—
IUGR, Bochum	↑	—	(↓) 0.08	—	↑	↓	—	—	—	—	—	—
OGTT 28–36 WGA					—	↓ ^a	↓ ^a	—				
Pre-post smoking 24–38 WGA					—	—	↓	—				

^a Reduced at third measurement time point.

Due to the fundamental limitations of ECG recordings, only a few acceptable recordings were available and did not allow a statistical analysis. They did however indicate similar qualitative results.

CTG recordings were not considered due to their lower time resolution and will be addressed in a subsequent study. The categories of long-term fluctuation amplitude and complexity can be considered as transferable to CTG data. In contrast, the short-term categories are not yet transferable since they are based on individual heart beat intervals that can so far not reliably be identified by the established CTG technology.

In all deviation data sets, we found that the HRV categories investigated here are correlated with the established HRV indices found in the original analyses of the data sets or similar analyses using other data sets.

- In fetuses of women doing aerobic exercise, all classical time and frequency domain fetal HRV indices were increased compared to fetal HRV of passive women at 36 WGA when fetuses were in the active sleep state (May *et al* 2010). Consistent with the initial report, the current re-analysis of this data set showed larger values of the category IAMP.
- Acute maternal cigarette smoking reduced fetal HRV (Graca *et al* 1991, Peterfi *et al* 2017). These results are in line with the reduced IAMP category in the present work.
- Maternal DHA supplementation increased SDNN, RMSSD, VLF, LF, (HF trend) (Gustafson *et al* 2013). It also increased fABAS, the maturation age score that includes indices of sAMP (pNN5), IAMP (ActAmp), and ICOMP (MSE3) (Hoyer *et al* 2018). Consistent with previously reported findings, the present work further expands our understanding, showing increased values of both fluctuation amplitude and complexity.
- In IUGR fetuses reduced HRV indices were shown that correspond to IAMP using CTG recordings (Nijhuis *et al* 2000). Decreased HRV complexity in IUGR fetuses has been described in CTG recordings (lyapunov exponent (LE) (Kikuchi *et al* 2008), Lempel Ziv complexity (LZC) and multiscale entropy (MSE) of approximate entropy (ApEn) and sample entropy (SampEn) (Ferrario *et al* 2009)) across the age range from 27 to 34 WGA. It should be noted that these indices of complexity, obtained from the CTG based heart rate signal, correspond to long-term behavior. Consistently, in the present work representatives of the IAMP and ICOMP categories were reduced. It should be noted, that furthermore the sAMP representative was decreased. Accordingly, fABAS that contains IAMP, sAMP and ICOMP was previously found reduced in IUGR fetuses (Hoyer *et al* 2013b).
- Reduced heart rate variability was observed in fetuses of mothers with GDM 120 min after the OGTT (Fehlert *et al* 2017). This is in accordance with the current finding of IAMP.

The choice of active sections (2F) is consistent with CTG recommendations and can be recommended in comparison to the more disperse and less defined non-state-classified recordings as well as the relatively rare quiet sleep (1F) sections. Our analyses of 1F and state-independent data (apart 5 min Bochum data) of all influencing factors were not outlined in the manuscript.

The elaborated minimal set of HRV indices was intended to be appropriate for routine overarching screening/monitoring. A resulting ‘polyscore’ (e.g. Steger *et al* (2019)) could identify suspect cases if one or more of the proposed category representatives is out of the normal range. This does not exclude the possibility that in identified suspect cases subsequent multivariate models using further indices such as power spectral ratios, α , or time

irreversibility indices, including those from different categories, may consider higher discriminatory complex interrelationships. However, those particular models are not helpful for the here proposed universal overarching monitoring.

Conclusion

The precise identification of fetal developmental disturbances by means of HRV indices requires the appropriate consideration of standardized representatives of HRV key characteristics under consideration of two factors, namely the maturation age and the disturbance of interest. For that purpose, the HRV categories short- and long-term fluctuation amplitude and short- and long-term fluctuation complexity integrate the most relevant HRV indices. The standardized use of representatives of these categories in a corresponding multivariate approach could help to establish a generally valid standardized diagnostic tool. We propose a multivariate screening discriminator that identifies changes in representatives of the categories IAMP, sAMP, ICOMP, sCOMP, and PATTERN.

This should be confirmed and possibly refined in subsequent analyses of independent data sets. Any contributing study center is welcome to collaborate.

Acknowledgments

AS, DH, US are supported by German Research Foundation: ‘Development of a clinic suitable marker of fetal autonomic maturation’ (DFG: Ho 1634/15-12, Schn 775/7-1). The building of the Jena Fetal Monitoring Data Base was furthermore supported by ‘Biomagnetic investigations of fetal autonomic and central nervous maturation and its disturbances due to intrauterine growth restriction and glucocorticoid administration (DFG: Ho 1634/12-2, Schn 775/2-3)’ and ‘Prenatal diagnosis indices of fetal developmental disturbances enabled by advanced signal identification techniques’ (Marie Curie Intra-European Fellowship, Proposal No. 237290).

KMG funding sources: The project investigating the effect of maternal exercise was supported by intramural grants from the Høglund Brain Imaging Center and Kansas City University of Medicine and Biosciences to KMG and Linda E May. The project investigating the effects of maternal smoking was supported by an Institutional Development Award (IDeA) to KMG from the National Institute of General Medical Sciences of the National Institutes of Health under grant number P20 GM103418. The randomized clinical trial (DHA) was supported by The Eunice Kennedy Shriver National Institute of Child Health and Development of the National Institutes of Health (R21 HD059019; KMG), registered at clinicaltrials.gov (NCT01007110). The content is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of General Medical Sciences, Child Health and Development or the National Institutes of Health.

DC is supported by Software AG Stiftung, Germany (DO-P 10545).

ORCID iDs

Dirk Hoyer  <https://orcid.org/0000-0003-4368-0053>

Kathleen M Gustafson  <https://orcid.org/0000-0003-3225-5086>

Silvia M. Lobmaier  <https://orcid.org/0000-0002-5696-6686>

Peter van Leeuwen  <https://orcid.org/0000-0003-2394-412X>

Dirk Cysarz  <https://orcid.org/0000-0001-8303-0261>

Hubert Preisl  <https://orcid.org/0000-0002-8859-4661>

References

- Amorim-Costa C, de Campos D A and Bernardes J 2017a Cardiotocographic parameters in small-for-gestational-age fetuses: how do they vary from normal at different gestational ages? A study of 11 687 fetuses from 25 to 40 weeks of pregnancy *J Obstet. Gynaecol. Res.* **43** 476–85
- Amorim-Costa C, Gaio A R, Ayres-de-Campos D and Bernardes J 2017b Longitudinal changes of cardiotocographic parameters throughout pregnancy: a prospective cohort study comparing small-for-gestational-age and normal fetuses from 24 to 40 weeks *J. Perinat. Med.* **45** 493–501
- Barker D J 1998 In utero programming of chronic disease *Clin. Sci.* **95** 115–28
- Bauer A, Kantelhardt J W, Bunde A, Barthel P, Schneider R, Malik M and Schmidt G 2006 Phase-rectified signal averaging detects quasi-periodicities in non-stationary data *Physica A* **364** 423–34
- Cysarz D, Porta A, Montano N, Leeuwen P V, Kurths J and Wessel N 2013 Quantifying heart rate dynamics using different approaches of symbolic dynamics *Eur. Phys. J.* **222** 487–500
- Cysarz D, Edelhauser F and Van Leeuwen P 2015 Strategies of symbolization in cardiovascular time series to test individual gestational development in the fetus *Phil. Trans. A* **373** 20140087
- David M, Hirsch M, Karin J, Toledo E and Akselrod S 2007 An estimate of fetal autonomic state by time-frequency analysis of fetal heart rate variability *J. Appl. Physiol.* **102** 1057–64

- Fehlert E et al 2017 Gestational diabetes alters the fetal heart rate variability during an oral glucose tolerance test: a fetal magnetocardiography study *BJOG* **124** 1891–8
- Ferrario M, Signorini M G and Magenes G 2009 Complexity analysis of the fetal heart rate variability: early identification of severe intrauterine growth-restricted fetuses *Med. Biol. Eng. Comput.* **47** 911–9
- FIGO (Federation Internationale de Gynecologie et d'Obstetrics) 2011 *Maternity Guidelines* (London, Germany: Federal Gazette, Institute for Quality and Efficiency in Health Care)
- Geirsson RT 1991 Ultrasound instead of last menstrual period as the basis of gestational-age assignment *Ultrasound Obst. Gyn.* **1** 212–9
- Graca L M, Cardoso C G, Clode N and Calhaz-Jorge C 1991 Acute effects of maternal cigarette smoking on fetal heart rate and fetal body movements felt by the mother *J. Perinat. Med.* **19** 385–90
- Gustafson K M, Carlson S E, Colombo J, Yeh H W, Shaddy D J, Li S and Kerling E H 2013 Effects of docosahexaenoic acid supplementation during pregnancy on fetal heart rate and variability: a randomized clinical trial *Prostaglandins Leukotrienes Essential Fatty Acids* **88** 331–8
- Haeckel E 1866 *General Morphology I: General Anatomy of Organisms. II. General Developmental History of Organisms* (G. Reimer Berlin) (in german)
- Hoyer D et al 2013a Fetal development of complex autonomic control evaluated from multiscale heart rate patterns *Am. J. Physiol. Regul. Integr. Comp. Physiol.* **304** R383–92
- Hoyer D, Tetschke E, Jaekel S, Nowack S, Witte O W, Schleussner E and Schneider U 2013b Fetal functional brain age assessed from universal developmental indices obtained from neuro-vegetative activity patterns *PLoS One* **8** e74431
- Hoyer D et al 2014 Fetal autonomic brain age scores, segmented heart rate variability analysis, and traditional short term variability *Frontiers Hum. Neurosci.* **8** 948
- Hoyer D, Schneider U, Kowalski E M, Schmidt A, Witte O W, Schleussner E, Hatzmann W, Gronemeyer D H and van Leeuwen P 2015 Validation of functional fetal autonomic brain age score fABAS in 5 min short recordings *Physiol. Meas.* **36** 2369–78
- Hoyer D et al 2017 Monitoring fetal maturation—objectives, techniques and indices of autonomic function *Physiol. Meas.* **38** R61–88
- Hoyer D, Schmidt A, Schneider U and Gustafson K 2018 Fetal developmental deviations reflected in a functional autonomic brain age score *Comput. Cardiol.* **45** 2018.009
- Kikuchi A, Unno N, Kozuma S and Taketani Y 2008 Detrended fluctuation analysis of heart rate variability in normal and growth-restricted fetuses *Gynecol. Obstet. Invest.* **65** 116–22
- Lempel A and Ziv J 1976 Complexity of finite sequences *IEEE Trans. Inf. Theory* **22** 75–81
- Lobmaier S M, Huhn E A, von Steinburg S P, Muller A, Schuster T, Ortiz J U, Schmidt G and Schneider K T 2012 Phase-rectified signal averaging as a new method for surveillance of growth restricted fetuses *J. Matern-Fetal Neonatal Med.* **25** 2523–8
- Maestri R et al 2007 Nonlinear indices of heart rate variability in chronic heart failure patients: redundancy and comparative clinical value *J. Cardiovasc. Electrophysiol.* **18** 425–33
- May L E, Glaros A, Yeh H W, Clapp J F 3rd and Gustafson K M 2010 Aerobic exercise during pregnancy influences fetal cardiac autonomic control of heart rate and heart rate variability *Early Hum. Dev.* **86** 213–7
- Nijhuis I J, ten Hof J, Mulder E J, Nijhuis J G, Narayan H, Taylor D J and Visser G H 2000 Fetal heart rate in relation to its variation in normal and growth retarded fetuses *Eur. J. Obstet. Gynecol. Reprod. Biol.* **89** 27–33
- Nijhuis J G, Prechtel H F, Martin C B Jr and Bots R S 1982 Are there behavioural states in the human fetus? *Early Hum. Dev.* **6** 177–95
- Pardey J, Moulden M and Redman C W 2002 A computer system for the numerical analysis of nonstress tests *Am. J. Obstet. Gynecol.* **186** 1095–103
- Peng C K, Havlin S, Stanley H E and Goldberger A L 1995 Quantification of scaling exponents and crossover phenomena in nonstationary heartbeat time series *Chaos* **5** 82–7
- Peterfi I, Kellenyi L, Peterfi L and Szilagyi A 2017 The short-term effect of smoking on fetal ECG *J. Matern Fetal Neonatal Med.* **26** 1–10
- Pillai M and James D 1990 The development of fetal heart rate patterns during normal pregnancy *Obstet. Gynecol.* **76** 812–6
- Porta A, Casali K R, Casali A G, Gnechchi-Ruscione T, Tobaldini E, Montano N, Lange S, Geue D, Cysarz D and Van Leeuwen P 2008 Temporal asymmetries of short-term heart period variability are linked to autonomic regulation *Am. J. Physiol. Regul. Integr. Comp. Physiol.* **295** R550–7
- Richman J S and Moorman J R 2000 Physiological time-series analysis using approximate entropy and sample entropy *Am. J. Physiol. Heart Circ. Physiol.* **278** H2039–49
- Schmidt A, Hoyer D and Schneider U 2018a Pattern-segmented heart rate variability analysis during fetal maturation *Computing in Cardiology* (Maastricht) vol 45 008
- Schmidt A et al 2018b Universal characteristics of evolution and development are inherent in fetal autonomic brain maturation *Auton. Neurosci.* **212** 32–41
- Schneider U, Frank B, Fiedler A, Kaehler C, Hoyer D, Liehr M, Hauelsen J and Schleussner E 2008 Human fetal heart rate variability—characteristics of autonomic regulation in the third trimester of gestation *J. Perinat. Med.* **36** 433–41
- Schneider U, Bode F, Schmidt A, Nowack S, Rudolph A, Doelcker E M, Schlattmann P, Gotz T and Hoyer D 2018 Developmental milestones of the autonomic nervous system revealed via longitudinal monitoring of fetal heart rate variability *PLoS One* **13** e0200799
- Steger A, Muller A, Barthel P, Dommasch M, Huster K M, Hnatkova K, Sinnecker D, Hapfelmeier A, Malik M and Schmidt G 2019 Polyscore of non-invasive cardiac risk factors *Frontiers Physiol.* **49** 1–10
- Stein P K 2005 Potential role of different components of heart rate variability for risk-stratification in critical care *Crit. Care Med.* **33** 2128–30
- TaskForce 1992 American college of chest physicians/society of critical care medicine consensus conference: definitions for sepsis and organ failure and guidelines for the use of innovative therapies in sepsis *Crit. Care Med.* **20** 864–74
- TaskForce 1996 Heart rate variability: standards of measurement, physiological interpretation and clinical use. Task Force of the European Society of Cardiology and the North American Society of Pacing and Electrophysiology *Circulation* **93** 1043–65
- Van den Bergh B R H et al 2017 Prenatal developmental origins of behavior and mental health: the influence of maternal stress in pregnancy *Neurosci. Biobehav. Rev.* (<https://doi.org/10.1016/j.neubiorev.2017.07.003>)
- Van Leeuwen P, Lange S, Bettermann H, Gronemeyer D and Hatzmann W 1999 Fetal heart rate variability and complexity in the course of pregnancy *Early Hum. Dev.* **54** 259–69
- Van Leeuwen P, Geue D, Lange S, Hatzmann W and Gronemeyer D 2003 Changes in the frequency power spectrum of fetal heart rate in the course of pregnancy *Prenat. Diagn.* **23** 909–16
- Van Leeuwen P, Gustafson K M, Cysarz D, Geue D, May L E and Gronemeyer D 2014a Aerobic exercise during pregnancy and presence of fetal-maternal heart rate synchronization *PLoS One* **9** e106036
- van Leeuwen P, Werner L, Hilal Z, Schiermeier S, Hatzmann W and Gronemeyer D 2014b Fetal electrocardiographic measurements in the assessment of fetal heart rate variability in the antepartum period *Physiol. Meas.* **35** 441–54